



Bioorganic Investigation of Encapsulated Cysteine Derivative into Polymeric Nanocarrier

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ABSTRACT

In this work, the copolymer-based synthesized Cysteine-loaded nanocarriers were prepared by a routine protocol, coprecipitation method. It is the first report to investigate the neuroprotective potential and biocompatibility of Cysteine derivatives loaded into poly(ethylene glycol)-block-poly(ϵ -caprolactone) methyl ether (PEG-b-PCL). The average size of the polymeric/empty NCs was 89 nm and for polymeric/Synthesized derivative of Cysteine was 126 nm. The Drug Loading efficiency was 81%. The concentration of Polymeric NCs was 2.1×10^{10} particles/mL and the zeta potential of polymeric/empty and polymeric/Synthesized derivative of Cysteine NCs -5 mV and -11 mV, respectively. Biological part of this work was investigated in the SH-SY5Y human neuroblastoma cell line using cell viability and toxicity assays. The concentration of polymeric NCs below 1×10^{10} particles/mL was described as a zero-point damageable for the cell line. Also, the Synthesized derivative of Cysteine encapsulated into polymeric NCs has more neuroprotective effect as compared to free Cysteine at lower concentration, and therefore, has a significant neuroprotective potential against Z-VAD-fmk and St-evoked SH-SY5Y cell damage.

Key words: Biocompatibility, Neuroprotective, Polymer, Biopolymer.

Introduction

Urbanization expansion, using radio-based services and rising average age of the world's population, has become the major factor to increase central nervous system (CNS) disorders. During the last decade, investigating biological systems based on biochemical mechanism of neuronal cell damage and biological models has been highlighted and considered by the researchers. (Ghasemi *et al.*, 2018; Nasseri *et al.*, 2018; Rabiee *et al.*, 2019b; Rabiee *et al.*, 2019c; Rabiee & Rabiee, 2019; Uttara *et al.*, 2009; Vafajoo *et al.*, 2018) It is vividly depicted that many inclusive diseases such as Parkinson, Huntington and Alzheimer crop up as a result of neurodegenerative processes, in addition the root mechanism of these diseases remotely related to the mitochondrial dysfunction and disrupted neuronal intracellular that cause calcium homeostasis which in turn leads to unusual activation of μ -calpain. As a matter of fact, the inhibition of hyper activity of calpain could lead to inhibition of calcium homeostasis and prevention of neuroprotective diseases

(Carragher, 2006; Deljoo *et al.*, 2019; Rabiee *et al.*, 2019a; Rabiee *et al.*, 2019; Szczech *et al.*, 2017). Without a shadow of a doubt, the effectiveness of the neuroprotective substances must take step progress, but it should be noted that the choice of these substances is very sensitive due to their chemical limitations which lead to peripheral toxicity and side effects (Svenson, 2012). In addition, the other issue which is remotely related to treatment of neurodegeneration is the incompetent delivery of drugs by the Blood-Brain Barrier (BBB). The central nervous system could be protected by biological membrane whose competent transport of chemical drugs and upholding the stability of the environment through Blood-Brain Barrier have become a great challenge.

Needless to say during the last decade, countless efforts have been made to implement prominent evolution in nano-scale generation of drugs in the diagnosis and treatment of diseases. In this regard, most scientists have focused on micro- and nanocarriers as drug delivery systems for these inclusive diseases such as Parkinson, Huntington and Alzheimer. In comparison to the regular and extracted-based natural drugs, especially coupled with nano-systems, it could be obvious to understand hopeful opportunities nano-systems would bring, *i.e.* improving *in vivo* bioavailability, boosting the efficiency of insoluble and mid soluble compounds. Moreover, reducing of side effects has been shown and of course they could be functionalized by chemical agents for targeting delivery (Chen *et al.*, 2016).

Recently, S-Allyl-L-Cysteine (PMI-CYSTEINE) (Figure 1) has introduced an agent of suppression of μ - and m -calpain activities followed by a bright promising neuroprotective compound (Imai *et al.*, 2014; Karimi *et al.*, 2018a; Karimi *et al.*, 2018b; Rabiee & Rabiee, 2018a, Rabiee & Rabiee 2018b). Previously, the PMI-CYSTEINE showed some crucial biological effects such as anticancer, (Thomson & Ali, 2003) antihepatotoxic (Kodai *et al.*, 2007) and neurotrophic activity in cultured rat hippocampal neurons (Moriguchi *et al.*, 1997). The result showed that PMI-CYSTEINE suppressed the TM-induced degradation of full length α -spectrin and remarkable suppression of μ - and m -calpain activities at higher concentrations.

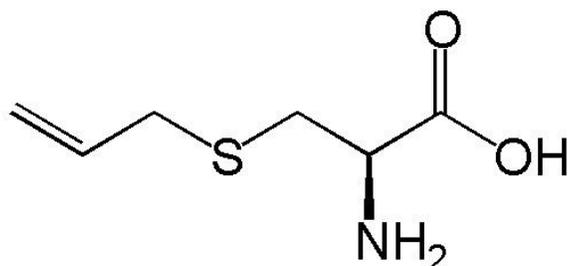


Figure 1. S-Allyl-L-Cysteine (PMI-CYSTEINE)

In this work, we have been focused on using Copolymer-based Synthesized derivative of Cysteine-loaded nanocarriers from coprecipitation method (Kayal & Ramanujan, 2010; Kharati *et al.*, 2018; Vafajoo *et al.*, 2018) at constant temperature followed by evaporation of an organic solvent. In addition, the biodegradable and biocompatible polycaprolactone-based copolymer (PCL) were used as a first attempt to encapsulate Synthesized derivative of Cysteine in the Polymeric nanocarrier to produce the polymer-based nanocarrier, and in this work, the biocompatibility of nanocarrier and neuroprotective potential of the encapsulated Synthesized derivative of Cysteine were evaluated in SH-SY5Y cells and MTT reduction for a first time.

Materials and methods

Materials

3-[4,5-dimethylthiazol-2-yl]-2,5-diphenyltetrazolium bromide (MTT), Fetal Bovine Serum (FBS), SH-SY5Y cell line human (Neuroblast from neuronal tissue), Poly(ethylene glycol)-block-poly(ϵ -caprolactone) methyl ether – PCL-b-PEG (PCL average Mw \approx 13,000 g/mol, PEG average Mw \approx 5,000 g/mol), Penicillin-Streptomycin solution (10,000 unit Penicillin and 10 mg Streptomycin/mL); Trypsin-EDTA solution (0.5 g porcine trypsin and 0.2 g EDTA); *N*-acetylcysteine (Grade \geq 99%); Staurosporine from *Streptomyces* sp.; Z-VAD-FMK; Lactate Dehydrogenase Activity Assay Kit (LDH) and Dulbecco's modified Eagle medium (DMEM) were purchased from Sigma-Aldrich Chemie GmbH, Germany.

Synthesis of PMI-CYSTEINE

The PMI-CYSTEINE was synthesized according the recently published paper (Kozma *et al.*, 2018). Briefly, 3,4,9,10-Perylene tetracarboxylic acid dianhydride (PDA) (0.5 mmol), *L*-CYSTEINE (1.05 mmol) and 1 g of imidazole were added into a Schlenk and heated at 120 °C for 4 h, while the colour turned from red to violet. The reaction mixture was filtered to eliminate the unreacted PDA, then was cooled, poured into water, and filtered. The recovered solid precipitate is PMI-Cys (15% yield).

Nanocarriers' preparation

Synthesized derivative of Cysteine-loaded Polymeric nanocarriers was prepared from coprecipitation method at constant temperature. The NCs were prepared by dissolving PMI-CYSTEINE (5 mg) in 2 mL of methanol/water (5/1), the PEG-b-PCL, in the determined amounts, was added to the same solution and sonicated for 3 min and, then, the solution was added drop wise to 10 mL water during 25 min. stirring was continued for 3 h to allow complete evaporation of the solvent. After that and in order to remove polymer aggregates, the NCs were filtered by a micro-filter with pore size of 1.5 μ m (Whatman® GD/X syringe filters) and the obtained suspension was centrifuged at 12,000 rpm for 40 min. Afterwards, the supernatant was alienated and the free PMI-CYSTEINE which remained in the supernatant was measured using HPLC method. The collected sediment was suspended in 1 mL deionized water and lyophilized using freeze-drier.

Loading efficiency and capacity

The loading efficiency (LE) and capacity (LC) of the NCs were determined by HPLC method as mentioned in preparing the NCs and calculated as follow:

$$LE(\%) = \frac{\text{Total amount of PMI – Cysteine added} - \text{Free SAC}}{\text{Total amount of SAC added}} \times 100$$

$$LC(\%) = \frac{\text{Total amount of PMI – Cysteine added} - \text{Free SAC}}{\text{Weight of nanoparticles}} \times 100$$

Nanocarrier' zeta potential determination

Zeta potential is one of the major physicochemical properties of NCs that determine the stability of NCs in aqueous medium. The zeta potential of nanocarriers was measured in water suspension by Laser Doppler Electrophoresis (LDE) technique using NANOPHOX Particle Size Analysis (Sympatec GmbH, Germany).

Nanocarrier' size analysis

NCs size distribution were investigated by dynamic light scattering (DLS) technique NANOPHOX Particle Size Analysis (Sympatec GmbH, Germany).

In vitro SH-SY5Y cell culture

SH-SY5Y cells from the cell line human neuroblast from neural tissue were grown in DMEM (with 10% Fetal Bovine Serum (FBS) and 0.1% Pen Strep solution). The cells were kept at 36°C (95% air and 5% CO₂). The cells were Trypsin-EDTA and seeded at a density of 6x10⁴ into 96-well plates. In addition, the cells were evaluated by LUNATM Automatic Cell Counter (Logos Biosystems).

Cell treatment

Initially, the cells were treated for 24 h with 20 µl of NCs suspension at different specific dilutions that were discussed in the discussion part. To proceed further investigation on neuroprotective potential, SH-SY5Y cells were co-treated with PMI-CYSTEINE-containing NCs at specific different dilutions and the polymer-cysteine (20 µM) alone and staurosporine (St) for comparison. Empty PEG-b-PCL NCs at dilution 1:4 and N-acetylcysteine antioxidant and pan-caspase inhibitor, Z-VAD-fmk (25 µM) were applied. First, 10 mM of PMI-CYSTEINE was dissolved in distilled water and stored at -20°C. 10 mM of staurosporine and 5 mM of Z-VAD-fmk solutions was prepared in a polar aprotic solvent such as DMSO. Final dilutions of St (15 µM), zVAD-fmk (1 mM) and PMI-CYSTEINE (1 mM) were prepared in distilled water. The final chemical mixtures were present in SH-SY5Y cell cultures (1% concentration for staurosporine and PMI-CYSTEINE, and 10% for NCs).

Cytotoxicity assay

SH-SY5Y cells were chosen due to the fact that our purpose was to investigate the PMI-CYSTEINE-loaded nanocarriers in neuropharmacology. This cell line which has been derived from a bone marrow biopsy of a neuroblastoma patient has been widely used in neurodegenerative and cytotoxic processes (Lopes *et al.*, 2010). To increase the authenticity and accuracy of the evaluation of the nanocarriers cytotoxicity, both MTT reduction and LDH release assays have been used to determine *in vitro* cell viability. The results of cytotoxicity test are summarized in Figure 2 and Figure 3. Cell viability and cell death assessments were investigated using LDH and MTT assays. Average concentration of each NCs, which were tested, was about 2×10¹⁰ particles/mL corresponding to about 5.5×10⁵ particles/cell. Both LDH and MTT assays were done after 24 h treatment with the specific agents.

Investigation of Cell viability

This assay in neuroprotection and biocompatibility studies was investigated by MTT assay. The exact procedure was described by (Liu *et al.*, 1997). In sum, the cells were incubated with 0.25 mg/mL MTT for 4 h at 37 °C and the reaction was stopped by adding a solution of 50% DMF and 20% SDS at pH 4.8. After 24 h, the amount of formazan product was determined by measuring the absorbance with a 96-well plate reader at a test wavelength of 570 nm and reference wavelength of 655 nm.

Statistical analysis

All of the data after normalization, were analyzed using Statistica software (StatSoft Inc., Tulsa, OK, USA).

Results and discussion

Preparation of Polymeric nanocarriers

In this work, the Polymeric NCs (PCL-b-PEG) were prepared from coprecipitation method (Kayal & Ramanujan, 2010) at constant temperature. The rate of solution addition to water was examined and the optimized rate was about 0.15 mL/min. NCs with about 2 mg/mL PEG-b-PCL (in the solution) were selected for this study because of the lowest polydispersity (PDI<0.2). Eventually during the evaporation of the organic solvent the Polymeric NCs were formed.

The average size of the PEG-b-PCL NCs without PMI-CYSTEINE which has been measured by DLS was about 108 nm with the PDI<0.2. The zeta potential of Polymeric NCs was -17 mV. The stability of NCs dispersion was investigated over 5 weeks too and approved the results.

Preparation of PMI-CYSTEINE loaded nanocarriers

The brief procedure of PEG-b-PCL PMI-CYSTEINE-loaded NCs preparation was described above. As a matter of fact, polymers as well as PMI-CYSTEINE (0.5 mg/mL) were dissolved in methanol/water with the Copolymer/drug ratio of 5:1. The average size of the PMI-CYSTEINE-loaded NCs that were measured by DLS was about 126 nm (Figure 2) and the polydispersity (PDI) index of PMI-CYSTEINE-loaded NC was <0.2. The zeta potential of PMI-CYSTEINE-loaded PEG-b-PCL NCs was -11 mV. Also the loading efficiency of PMI-CYSTEINE into NC was examined and the result shows 81% with the entrapment efficiency of about 93%. In addition, the PMI-CYSTEINE release at 24 h was 46.9% with the correlation coefficients of 0.8520, 0.9492 and 0.6926 for zero order, Higuchi and Hixson-Crowell, respectively. The stability of PMI-CYSTEINE-loaded NCs was examined for 5 weeks which was verified by repeated measurements of their zeta potential.

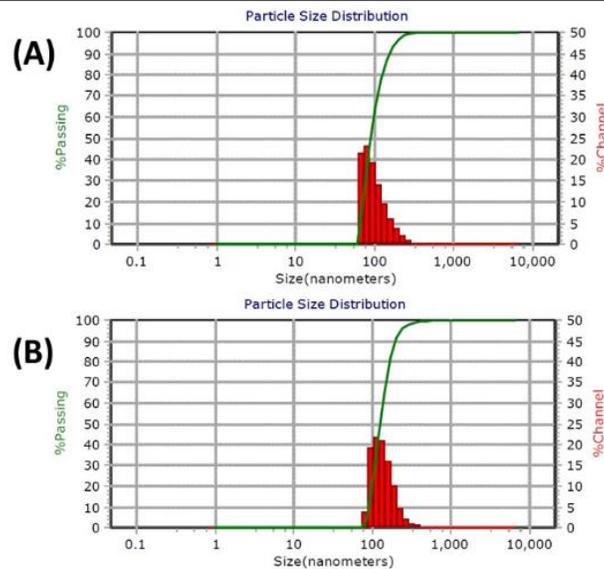


Figure 2. Size distribution of the polymeric NC and Synthesized derivative of Cysteine loaded polymeric NC measured by DLS technique (A) and (B) respectively.

The detailed characterization of NCs are shown in Table 1.

Table 1. The composition and detailed characterization of NCs

Sample	The average size (nm)	PdI	Zeta Potential (mV)
PEG-b-PCL/empty	89	0.161	-5
PEG-b-PCL/PMI-CYSTEINE	126	0.188	-11

Investigation of Biocompatibility

After 24 hours, treatment evoked significant toxicity (2-4.5-fold increases in LDH level) as depicted in Figure 3 as well decrease in cell viability, and 18% decrease in MTT assay, as shown in Figure 4.



Figure 3. LDH Release of empty and PMI-CYSTEINE containing polymeric NCs, (one way ANOVA followed by Tukey's test ($P < 0.001$ vs. vehicle-treated cells; and $P < 0.001$ N-1 vs. PMI-CYSTEINE-treated cells)).

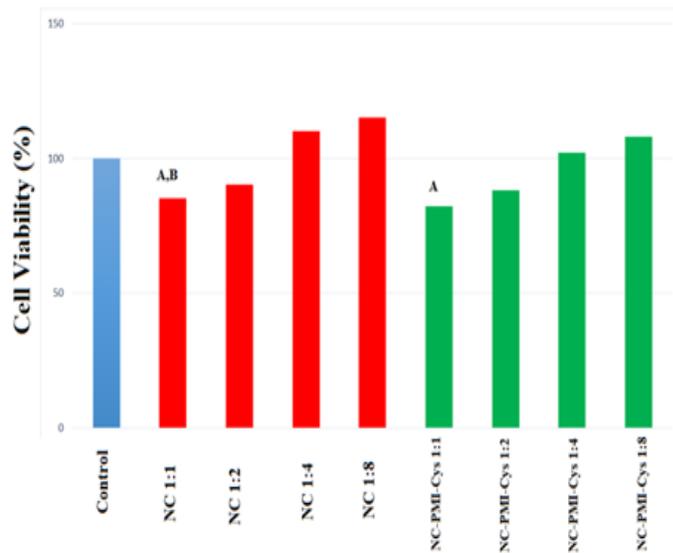


Figure 4. Cell viability (MTT Reduction assay) of empty and PMI-CYSTEINE containing polymeric NCs, (one way ANOVA followed by Tukey's test (A : $P < 0.001$ vs. vehicle-treated cells; B : $P < 0.001$ N-1 vs. PMI-CYSTEINE-treated cells))

In this case, Polymeric NCs at dilution 1:1 have a slightly more toxic effect in both used assays for PMI-CYSTEINE-loaded NCs to compare with empty copolymer. As it has been depicted in Figure 3, the cytotoxic effect was decreased by increasing the dilutions of NCs, so the concentration of Polymeric NCs below 1×10^{10} particles/ml can be deliberated as a safe concentration for the cell line.

Neuroprotection studies

Initially, researcher's introduced the programmed cell death to describe ostensibly pre-determined pattern in which specific cells die during a procedure, which has a crucial role in the development of the nervous system (Ito *et al.*, 2003; Ueda *et al.*, 2002; Zalucki *et al.*, 2017). There is another mechanism to describe neuronal cell loss under different neurodegenerative conditions in which apoptotic processes and also oxidative stress have a decisive role (Bredesen *et al.*, 2006). Since the therapeutic effect of PMI-CYSTEINE was determined in various models of neurodegenerative disease, such as Alzheimer, (Javed *et al.*, 2011) and of course the antioxidant effect and related mechanism were confirmed, (Colín-González *et al.*, 2012; Niedzielska *et al.*, 2016), we have used the model of pro-apoptotic factor staurosporine-evoked cell damage in SH-SY5Y cell line. This effort was to tackle on the issue of neuroprotective potential of PMI-CYSTEINE loaded NCs in comparison to the effect of PMI-CYSTEINE empty to have steps coming along with the recent research. The result of MTT reduction assay showed about 18% neuroprotective effect of Z-VAD-fmk as model inhibitor and about 12% neuroprotective effect of PMI-CYSTEINE against St-evoked SH-SY5Y cell damage which has been depicted in Figure 5. In addition, 22% protection for PMI-CYSTEINE loaded Polymeric NC at dilution 1:8 in St Model of cell damage is clear and the amazing result is the PMI-CYSTEINE loaded Polymeric NC at any dilution has not shown more toxicity than staurosporine.

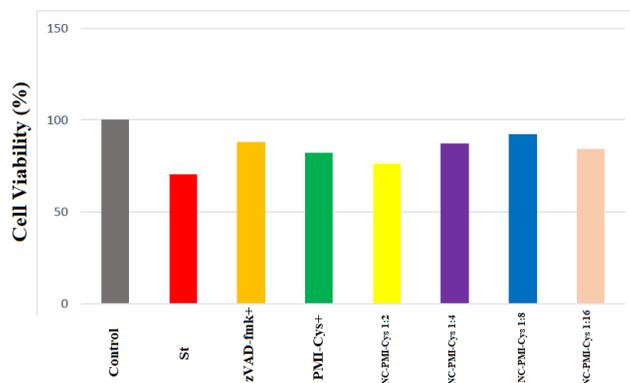


Figure 5. Neuroprotective effects of polymeric NCs containing PMI-CYSTEINE against staurosporine (St). (one way ANOVA followed by Tukey's test ($P < 0.001$ vs. vehicle-treated cells; $P < 0.001$ vs. St-treated cells))

A striking result which could be the PMI-CYSTEINE encapsulated into Polymeric NC compared with free PMI-CYSTEINE would shows 10% more neuroprotective effect and it means the PMI-CYSTEINE encapsulated into Polymeric NC compared with free PMI-CYSTEINE can gives considerable results.

Conclusion

The polymeric NC has been prepared from coprecipitation method at constant temperature followed by evaporation of an organic part of the solvent. This method was applied to investigate the neuroprotective action of PMI-CYSTEINE, which is encapsulated into polymeric NC. This work is the first report to encapsulate PMI-CYSTEINE in the polymeric NC representing some critical facts of the neuroprotective action of PMI-CYSTEINE. The results from biocompatibility tests indicated that polymeric NCs at dilution 1:1 have been showing a slightly more toxic effect in both used assays for PMI-CYSTEINE-loaded NCs as compared to the empty one. However, the cytotoxic effect was decreased by increasing the dilutions of NCs, so it was optimized to the concentration of Polymeric NCs which could be mentioned as a safe concentration for the cell line. The results from Neuroprotection studies indicated that PMI-CYSTEINE was encapsulated into Polymeric NCs as compared to the free PMI-CYSTEINE which would show more neuroprotective effect and give the same neuroprotective effect as a free PMI-CYSTEINE at lower concentration. Thus, the MTT assay showed that PMI-CYSTEINE loaded in PEG-b-PCL NCs has a significant neuroprotective potential against Z-VAD-fmk and St-evoked SH-SY5Y cell damage. This work represented important results which may be considered by more advanced researches. In fact, in future, we want to focus on the *in vivo* strategies and optimizations based on the stability, tissue interactions and reducing the side effects.

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